Probabilistic risk assessment of gold nanoparticles after intravenous administration by integrating in vitro and in vivo toxicity with physiologically based pharmacokinetic modeling

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Prostate cancer is a leading cause of cancer-related mortality in men. Recent advancements in nanotechnology have identified promising engineered nanomaterials (or nanoparticles, NPs) for various applications, including disease diagnostics and therapeutics. Amongst the myriad of NPs available, gold nanoparticles (AuNPs) have great potential for wide applications in nanomedicine due to their unique physical, chemical, and optoelectronic properties. Specifically, AuNPs can serve as either diagnostic or therapeutic agents for tumors or rheumatoid arthritis, or as carriers for delivery of drugs, antigens, peptides, and genetic materials (Arvizo et al. 2012; Jain et al. 2012). The use of AuNPs inevitably increases the likelihood of unintentional low-dose environmental exposure, occupational exposure, and intentional high-dose exposure for medical purposes; raising concern about the potential short-term and long-term adverse effects on human health (Khlebtsov and Dykman 2011). Despite these exposures, the potential risk of AuNPs has not been well characterized.

Numerous in vivo and in vitro studies have investigated the potential toxicity of AuNPs. Zhang et al. (2011) reported that exposure to 10 and 60 nm polyethylene glycol (PEG)-coated AuNPs after intraperitoneal injection caused significant increase in alanine transaminase and aspartate transaminase and decrease in creatinine, suggesting liver and kidney damage in mice, while 5 and 30 nm AuNPs caused relatively lower toxicity, implying...
size-dependent toxicity. Cho et al. (2009) demonstrated dose-dependent liver toxicity in mice exposed to 13 nm PEG-coated AuNPs after intravenous injection. *In vitro* studies based on human- or animal-derived cells have also suggested dose-dependent cytotoxicity of AuNPs (Pernodet et al. 2006; Mannerström et al. 2016). Additionally, a bio-corona which forms instantly upon contact with biological fluids as biomolecules attaching to the NP surface has also been shown to modulate AuNPs cellular uptake and toxicity (Westmeier et al. 2016; Chandran et al. 2017). One challenge in this field is that the existing AuNP toxicity studies have used different study designs (cell types, media composition, particle characterization methods, and biomarkers of cytotoxicity) with different types of AuNPs (i.e. varied in size, shape, dose, and surface functionalization) that prevent integrating available experimental evidence into a comprehensive systematic evaluation.

To conduct such an integrated risk assessment of AuNPs, we determined the dose-dependent cytotoxicity of different sizes (40 and 80 nm) of AuNPs coated with PEG, branched polyethyleneimine (BPEI), or lipoic acid (LA) that were pre-incubated with human plasma proteins (HP) or human serum albumin (HSA) (to form defined protein coronas), or without pre-incubation with proteins (bare) in four human cell types, including hepatocytes (Choi et al. 2017), umbilical vein endothelial cells (HUVEC) (Chandran et al. 2017), renal proximal tubule epithelial cells (HRPTEC) (Ortega et al. 2017), and keratinocytes (Li and Monteiro-Riviere 2016). Additionally, we used our recently developed physiologically based pharmacokinetic (PBPK) model for AuNPs in mice and rats that had been successfully extrapolated to humans (Lin et al. 2016a, 2016b; Lin et al. 2017). This model allows one to conduct *in vitro* to *in vivo* extrapolation (IVIVE) and cross-species extrapolation of the dosimetry and toxicity of AuNPs, thereby providing a basis for quantitative risk assessment.

The objective of this study was to conduct an integrated and probabilistic risk assessment of AuNPs in humans after intravenous (IV) administration, which is the most commonly used administration route in animal studies and in humans for biomedical application. Specifically, this study aimed to (i) conduct dose–response relationship analyzes based on our reported *in vitro* toxicity studies, (ii) implement the validated human PBPK model incorporating Monte Carlo simulation to estimate internal dosimetry under various exposure scenarios, (iii) characterize the potential risk of AuNPs under different exposure scenarios using a Bayesian-based probabilistic risk assessment framework (NRC 2009; EPA 2014; Cheng et al. 2016), and (iv) explore several points of departure (PODs) for AuNP exposure by reconstructing exposure dosimetry based on either *in vitro* or *in vivo* biological responses.

**Materials and methods**

**Modeling framework**

To assess the potential risks of AuNPs to humans, we applied a probabilistic approach based on US EPA guidelines (NRC 2009; EPA 2014). Figure 1 represents a conceptual framework depicting the general process in probabilistic risk assessment that contains four critical elements; hazard identification, dose–response analysis, exposure analysis, and risk characterization. In addition, this study estimated the human equivalent dose (HED) associated with reported or estimated PODs (NOAEL and LOAEL [no and lowest observed adverse effect levels, respectively] and EC$_5$ and EC$_{10}$ [exposure concentrations causing 5% and 10% maximum cell death, respectively]) based on *in vivo* or *in vitro* toxicity studies using the human PBPK model. We term this process exposure reconstruction (detailed below).

**Hazard identification**

To determine the potential toxicity of AuNPs, we conducted a comprehensive evaluation of the effects of various types of AuNPs on the viability of different human cell types, including hepatocytes (Choi et al. 2017), HUVEC (Chandran et al. 2017), HRPTEC (Ortega et al. 2017), and keratinocytes (Li and Monteiro-Riviere 2016) using the same AuNPs. The experimental designs of these studies were similar. In brief, cells were exposed for 24 h to different concentrations (e.g. 0–400 µg/mL for hepatocytes) of spherical Biopure™ 40 or 80 nm AuNPs coated with PEG (neutral), BPEI (positive), or LA (negative) (nanoComposix, San Diego, CA) that were pre-incubated with HP or HSA, or without pre-incubation with proteins (bare). Cell viability was
determined using the alamarBlue assay as previously described (Monteiro-Riviere et al. 2009). Note that only the 40 and 80 nm AuNPs coated with BPEI and BPEI-HP were found to cause significant cytotoxicity in selected cell types.

Besides toxicity data from our own group, we also included data from an independent study in which the apoptotic effect of AuNPs on human neutrophils (polymorphonuclear neutrophil cells, PMNs) was determined (Noël et al. 2016). Briefly, PMNs
were exposed to different concentrations of PELCO® BioPure™ 20 or 70 nm AuNPs (Ted Pella, Redding, CA) for 24 h and apoptosis was assessed by counting Hema 3-stained PMN with light microscopy. Additional information on the experimental designs and physicochemical properties of studied AuNPs is provided in the studies listed in Supplementary Table S1. The cytotoxicity data from selected studies were used for subsequent dose–response analyzes.

**Dose–response assessment**

To investigate dose dependency of AuNP-induced cytotoxicity, several commonly applied quantal models, including exponential, Weibull, Logistic, and Hill models were adopted to reconstruct dose–response relationships (WHO 2009; EPA 2012) (Figure 1B).

\[
\begin{align*}
\text{Exponential: } P(E|C) &= E_{\text{max}} - \exp(-\beta \times C) + E_{\text{min}}, \\
\text{Weibull: } P(E|C) &= E_{\text{max}} \exp\left(-\frac{(E_{\text{min}} + (\beta \times C)^n)}{E_{\text{max}} - E_{\text{min}}}\right), \\
\text{Logistic: } P(E|C) &= \frac{E_{\text{max}} - E_{\text{min}}}{1 + \exp\left(\alpha - \beta \times C\right)} + E_{\text{min}}, \\
\text{Hill: } P(E|C) &= \frac{(E_{\text{max}} - E_{\text{min}}) \times C^n}{(E_{C50} + C^n)} + E_{\text{min}},
\end{align*}
\]

where \( P(E|C) \) is the conditional probability representing the probability that a certain effect (i.e. a certain fraction of cell death) may occur at a given AuNP exposure concentration, \( E_{\text{min}} \) and \( E_{\text{max}} \) represent minimum and maximum fractional cell death, respectively, \( E_{C50} \) is the exposed concentration leading to half maximum cell death fraction (\( \mu g/ml \)), \( \alpha \) is the parameter indicating location in the Logistic model, \( n \) is the exponent parameter in the Weibull model, and \( \beta \) (as in exponential, Logistic, and Weibull models) and \( n \) (referred to as the Hill coefficient in Hill model) are slope factors that determine the overall shape of the dose–response curve. A commercial software package TableCurve 2D™ (Version 5.1.2, Systat Software Inc., San Jose, CA) was employed to perform nonlinear curve fitting to derive the optimal fitting model based on the goodness-of-fit (determination of coefficient, \( r^2 \)) and to determine the parameter values using the least-square method with a \( p \) value of <0.05 considered as statistically significant.

In this study, we employed the administered/applied in vitro concentrations in the dose–response analyzes of the selected in vitro toxicity data. Multiple studies have shown that the delivered dose is a more appropriate dose metric than the administered dose/concentration in the interpretation of in vitro toxicity data for NPs (Hinderliter et al. 2010; Cohen et al. 2014; DeLoid et al. 2017). In this regard, we also applied a commonly used model (i.e. the in vitro sedimentation, diffusion, and dosimetry [ISDD] model) to predict the deposited fractions of AuNPs after different times of exposure based on the experimental condition in Choi et al. (2017). The results showed that at 24 h post-exposure to bare AuNPs, up to 100% (i.e. 83–100%) of the applied dose would be deposited to the bottom of the cell culture plate (Supplementary Table S2). Ideally, it would be optimal to use the ISDD model-predicted delivered dose to conduct the dose–response analysis. However, the ISDD model-predicted delivered dose is typically in the unit of pg NPs per cell (pg/cell) or number of NPs per cell. At this stage, it cannot be smoothly integrated with our PBPK model simulation result, which is typically in a unit of \( \mu g/g \) tissue (\( \mu g/g \)), representing the overall concentration of NPs in the organ. In order to fully integrate ISDD model with PBPK model, we will need a more detailed mechanistic model that simulates the distribution of NPs at both the cellular and organ level, so that we can use the PBPK model to simulate the concentration of NPs in individual cells. This is a future research direction once additional data become available.

**Exposure analysis**

To quantify internal exposure concentrations of AuNPs in human target tissues or organs after IV administration, the previously validated human PBPK model extrapolated from rats was implemented (Lin et al. 2016a). In brief, the human PBPK model contained seven compartments; including plasma, lungs, liver, kidneys, spleen, brain, and rest of body (Supplementary Figure S1). To better describe the biodistribution of AuNPs, a membrane-limited model structure incorporating endocytosis of AuNPs from plasma to tissue phagocytic cells (PCs) was adopted (Lin et al. 2016a, 2016b). Except for plasma and brain, all compartments were divided into three sub-compartments as capillary blood, tissue, and PCs. All the physiological and AuNP-specific parameters used in the validated
human PBPK model were kept the same as in the original model and provided in our previous work (referred to Supplementary Tables 2 and 3 in Supporting Information from Lin et al. 2016a). The complete human PBPK model code is provided in the Supplementary Material.

A wide range of IV administered doses (0.001–100 mg/kg) that have been applied in animal studies (mice or rats) (Khlebtsov and Dykman 2011; Lin et al. 2015) was selected to derive the associated human doses in order to predict internal tissue exposure concentrations in humans. To better determine the levels of AuNPs in human tissues and to assess the potential risks after IV administration with different dose levels, we categorized the animal IV dosages into three dosing windows as low (<0.1 mg/kg), medium (0.1–10 mg/kg), and high (>10 mg/kg), respectively based on the frequency of a specific dosing window as reported in Khlebtsov and Dykman (2011). This categorization only applies to IV administration in the present study and it is consistent with the dose stratification in our earlier study (Lin et al. 2016a). Among the reported animal IV doses included in Khlebtsov and Dykman (2011), the low-to-medium IV dose range was commonly used and only a few studies used the high IV dose window. Since we utilized a species-specific and physiologically based modeling approach, we directly incorporated the animal doses into the human PBPK model to assess the potential risks in humans exposed to doses used in animal studies. Additionally, in clinical pharmacology, it is a common practice to use an allometric approach in the translation of doses between two different species and estimation of a more accurate starting dose for clinical trials, provided considering species differences in pharmacokinetic parameters such as clearance and volume of distribution (Sharma and McNeill 2009). Therefore, we also assessed the potential risks in humans exposed to human doses (HD) that were scaled from animal doses (AD) based on reported conversion factors ($K_{m}$) using the following equation (Sharma and McNeill 2009; Nair and Jacob 2016),

$$HD \text{ (mg/kg)} = AD \text{ (mg/kg)} \times \left(\frac{K_{m,m} \text{ or } K_{m,r}}{K_{m,h}}\right). \quad (5)$$

where $K_{m,m}$, $K_{m,r}$, and $K_{m,h}$ represent conversion factors associated with the body surface area and body weight in mice (20 g, $K_{m,m} = 3$), rats (250 g, $K_{m,r} = 7$), and humans (70 kg, $K_{m,h} = 37.8$), respectively (Nair and Jacob 2016).

In this study, we applied two different approaches to derive the human doses for assessing the potential risks in order to compare the differential risks between our PBPK approach and the PBPK+ allometric approach. The allometric approach is commonly used for small molecular drugs, but its application for NPs has not been validated. Additional studies are needed to test whether the allometric approach is applicable or necessary to NPs. Supplementary Table S3 summarizes IV administered dosages of AuNPs applied in animal studies and the associated scaled dosages that were implemented in human PBPK modeling. Results of both approaches were compared and discussed below.

The random-sampling Monte Carlo simulation technique was implemented while scaling low, medium, and high AD (LAD, MAD, and HAD) to the associated low, medium, and high HD (LHD, MHD, and HHD) in order to consider variability and uncertainty within each dosing range (Bois et al. 2010; Cheng et al. 2016; Shi et al. 2016). Monte Carlo simulation was performed with 10,000 iterations via the software Crystal Ball® (Version 11.1.2.4, Oracle Corporation, Redwood Shores, CA) as an add-in within Microsoft Excel (Version 2016) to ensure the stability of input dose distribution profiles. Specifically, the minimum and maximum values of a specific AD or HD range were assigned as 1st and 99th percentile of a lognormal (LN) distribution (i.e. to define the assumption in Crystal Ball) to generate the mean dose and the standard deviation (SD) of a particular dose window (i.e. to generate the forecast in Crystal Ball). The LN distribution was found to be the optimal distribution based on the K–S value of the Kolmogorov–Smirnov test. This same procedure was applied to estimate the mean and SD values for the LAD, MAD, HAD ranges (non-scaled), as well as the LHD, MHD, and HHD ranges (allometry-scaled) (Figure 1(C) and Supplementary Table S3).

Since our PBPK model only contains plasma, lungs, liver, kidneys, spleen, brain, and rest of body compartments, we could not directly estimate internal concentrations of AuNPs in endothelial cells and keratinocytes using the model. We alternatively estimated internal concentrations in venous plasma...
and rest of body as surrogates for internal concentration in endothelial cells and keratinocytes, respectively. This was done because endothelial cells are in direct contact with the plasma and the skin is a major part of the rest of body compartment in our model. We acknowledged that this will introduce some uncertainty to our analysis. A more detailed mechanistic PBPK model would help improve our analysis, but it would require additional data for model construction, which is a future research direction.

Maximum internal exposure concentrations (C\text{max}) in venous plasma, liver, kidney, and rest of body were then estimated by incorporating the LN distributed ADs and HDs into the human PBPK model using Berkeley Madonna\textsuperscript{TM} (Version 8.3.23, University of California at Berkeley, CA). There is no a built-in function in Berkeley Madonna to perform Monte Carlo simulation for LN distribution. Since the lognormal distribution is a continuous probability distribution of a random variable whose logarithm is normally distributed, we applied the inverse natural logarithmic transformation of the “NORMAL” function to produce lognormally distributed random numbers based on our recently published method (Li et al. 2017a). After incorporating the LN distributed doses into the human PBPK model, 1000 simulations were performed in Berkeley Madonna to compute internal concentrations in liver, kidney, venous plasma, and rest of body (mean ± SD) underlying different exposure scenarios. Here we simulated only 24-h biodistribution data according to the exposure durations in selected in vitro studies. Finally, we performed 10 000 Monte Carlo simulations using Crystal Ball to select the optimal distribution based on Kolmogorov–Smirnov statistics and to estimate associated probability density functions (PDFs) for maximum internal exposure concentrations (i.e. the frequency or probability of a specific internal concentration to occur).

**Risk characterization**

To further characterize the human exposure risk after IV administration of AuNPs, this study implemented a Bayesian-based probabilistic risk assessment model by linking the AuNP-PBPK exposure model with the dose–response model. Specifically, the optimized distribution profiles as well as PDFs of maximum internal AuNP exposure concentrations in humans under various dosing ranges, P(C) (i.e. the prior probability), were estimated based on the simulated results obtained from the human AuNP-PBPK model (Figure 1(C)). A likelihood P(E|C) (i.e. the likelihood that a certain endpoint (e.g. fractional cell death) may occur at a given exposure concentration of AuNPs) was obtained from the best-fitted dose–response profiles (Figure 1(B)). This study then added up the PDF of the prior probability to estimate the cumulative distribution function (CDF) for following analyzes using the Bayesian inference.

Followed by the Bayesian inference, a CDF describing cumulative risk probability of a specific extent of human cell death endpoint to occur at a particular AuNP exposure concentration corresponded to a specific cumulative probability, was derived by combining both prior probability (Figure 1(C)) and likelihood (Figure 1(B)), resulting in a posterior probability, P(C|E) (Figure 1(D)), estimate:

\[
P(C|E) = P(C) \times P(E|C).
\]

(6)

This analysis then converted cytotoxicity–cumulative risk probability profile into exceedance risk profile. The exceedance risk profile represents the probable exceedance probability for a specific cell death fraction to occur at a particular exposure dose/concentration and can be calculated as “1 – CDF”, e.g. an exceedance probability of 0.5 suggests there is 50% chance (i.e. likely) for cellular death to exceed a particular fraction at a given exposure.

**Exposure reconstruction using in vitro to in vivo extrapolation approach**

Two PODs estimated from in vitro dose–response relationships using the Hill model (EC\text{5} and EC\text{10}) were considered for estimating the associated administered external dosing levels in humans (i.e. HED). Specifically, this study first estimated mean and 95% confidence interval (CI) values of EC\text{5} and EC\text{10} for different human cell types via TableCurve 2D. Berkeley Madonna was then applied to estimate the exact administration dosages that would result in maximum target organ concentrations that were equal to mean and 95% CIs of EC\text{5} and EC\text{10} using the human PBPK model. We termed the process of estimating administered HEDs through the human PBPK model based on PODs derived from the
in vitro dose–response models as reverse dosimetry analysis or exposure reconstruction.

**Exposure reconstruction using animal-to-human extrapolation approach**

This study also estimated the HEDs associated with reported PODs (e.g. NOAEL or LOAEL) based on endpoints previously calculated from animal studies (Cho et al. 2009; Balasubramanian et al. 2010). Explicitly, Balasubramanian et al. (2010) performed an in vivo study to investigate biodistribution and toxicity after single IV injection of 0.01 mg/kg AuNPs in rats for up to 2 months, and observed significant changes on the expression of genes related to detoxification, lipid metabolism, and cell cycle effects in target organs liver and spleen. Among the published toxicity studies of AuNPs investigating the adverse outcomes in rodents, this is the study that reported significant toxicity at the lowest administered dose. Therefore, we considered this dose as LOAEL for the endpoint of gene expression changes. Additionally, Cho et al. (2009) conducted a biodistribution study with IV administered dosages ranging from 0.17 to 4.26 mg/kg and used a TUNEL (terminal deoxynucleotidyl transferase-mediated dUTP nick end-labeling) assay to detect apoptosis in mouse liver tissue. The NOAEL and LOAEL were reported to be 0.85 and 4.26 mg/kg, respectively. The reported NOAEL and/or LOAEL were then incorporated into our published mouse or rat PBPK model (Lin et al. 2016a) to estimate the corresponding maximum liver concentration. Assuming that the same effect in humans would occur if the target organ liver concentration in rodents is the same as in humans, HEDs associated with reported PODs in rodents can then be determined based on the human PBPK model through a reverse dosimetry analysis (WHO 2010).

**Results**

**In vitro dose–response relationships**

Our earlier study (Choi et al. 2017) showed that only AuNPs coated with BPEI with or without HP protein coronas caused significant cytotoxicity in human hepatocytes. To determine the optimal dose–response model for describing AuNP exposure concentration corresponded cellular death in hepatocytes, the differences in goodness-of-fit ($r^2$ values) and parameter estimates of constructed models were compared and summarized in Supplementary Table S4. Among the constructed dose–response relationships, the Hill model has superior goodness-of-fit for hepatocyte toxicity data compared to other models, including exponential, Weibull, and Logistic models (Supplementary Table S4 and Figure S2). In addition, the Hill model can describe cytotoxic response at both low and high exposure concentrations more adequately than other models. Therefore, we selected Hill model to describe an individual in vitro dose–response relationships afterwards. Figure 2(A–D) demonstrated that the Hill model adequately characterized the relationship between the exposure concentration of AuNPs and the corresponding observed cytotoxicity in hepatocytes ($r^2 = 0.90–0.99$, $p < 0.001$) (Table 1). Among the studied AuNPs of different sizes and surface coatings, 40 nm bare AuNP-BPEI is the most toxic with $E_{50}$ estimated to be 185 μg/ml (95% CI: 167–203 μg/ml) and >90% cell death under maximum exposure concentration of 400 μg/ml (Figure 2(A)). In contrast, AuNP-BPEI coated with HP coronas had substantially lower cytotoxicity with $E_{50}$ (mean ± SE) estimated to be 273 ± 23 and 395 ± 5 μg/ml for 40 and 80 nm AuNP-BPEI-HP, respectively (Figure 2(C,D), Table 1).

For other human cells, 40 and 80 nm bare AuNP-BPEI-induced cytotoxicity can be well characterized with the Hill model as well ($r^2 = 0.91–0.98$, $p < 0.001$) (Figure 3(A–E), Table 1). Based on the fitted results, AuNP-BPEI-induced cell death fractions were similar among human keratinocytes, HUVEC, and HRPTEC cells with $E_{50}$ estimates ranging from 62 to 81 μg/ml and with 70–81% cell death under 100 μg/ml bare AuNP-BPEI exposure (Figure 3(A–E), Table 1). Additionally, 40 nm bare AuNP-PEG caused relatively low, but quantitable cytotoxicity to HUVEC compared to bare 40 nm AuNP-BPEI with cell death fraction estimated around 21% under 200 μg/ml bare AuNP-PEG exposure (Figure 3(F), Table 1). For PMNs, instead of fixing $E_{\text{max}}$ to 1, optimally fitted $E_{\text{max}}$ estimates of 0.60 and 0.83 were adopted because observed toxicity data close to 100% cell death were not available. The Hill model provided statistically significant and acceptable fitting results with Hill coefficients $n$ estimated to be 0.29 ($r^2 = 0.63$, $p < 0.001$) and 0.47 ($r^2 = 0.81$, $p < 0.001$), respectively. However, the dose-dependence in
AuNP-induced PMN toxicity was not obvious \((n < 1)\) (Figure 3(G,H), Table 1).

**External and internal exposure concentration estimates**

Figure 4(A–C) displays human IV dosages associated directly with animal dosing levels (LAD, MAD, and HAD) (i.e. without scaling). Based on Monte Carlo simulation results, the median dose estimates for LAD, MAD, and HAD were \(\sim0.06, 0.8, \text{ and } 33 \text{ mg/kg}\), respectively. Whereas for the scaled LHD, MHD, and HHD, the estimated median values ranged from nearly 0.01 to 2.6 mg/kg (Supplementary Figure S3).

Simulated maximum concentrations of AuNPs in target tissues or organs (liver, kidney, venous plasma, and rest of body) within 24 h after low, medium, and high IV administration can be well depicted with LN distributions (Figure 4(D–O)). For humans directly receiving LAD, MAD, and HAD, the maximum internal concentrations were observed in venous plasma with geometric means (GMs) of LN distribution estimated to be around 0.9, 10.8 and 418.8 \(\mu\text{g/ml}\), respectively (Figure 4(E,I,M)). Whereas for people receiving the high scaled dosing level, maximum concentration occurred at 24 h in liver with GM and geometric standard deviation (GSD) estimated to be 45.3 \(\mu\text{g/g}\) and 1.1, respectively (Supplementary Figure S3). The lowest \(C_{\text{max}}\) were found in rest of body among all selected tissues or organs with GMs estimated to be around 0.01–1.5 \(\mu\text{g/g}\) (Supplementary Figure S3).

Comparing all distribution profiles, medium and high dosage-based internal concentration distribution profiles more likely followed a normal rather than lognormal distribution with GSDs approximating 1 (Figure 4(H–O) and Supplementary Figure S3).

**Risk estimation**

By linking maximum internal concentrations estimated from the human PBPK model with
constructed in vitro dose–response models, the human exposure risk to AuNPs with different sizes and surface coatings can be estimated. Specifically, the results showed that there was a 50% risk probability for people receiving low and medium nonscaled AuNP IV doses to have more than 0.001–3.4, 0.02–1.0, 0.003–0.1, and 1.7–8.9% cell death in hepatocytes (Figure 5(A,B)), HUVEC (Figure 5(D,E,G,H)), HRPTEC (Figure 5(J,K)), and keratinocytes (Figure 5(M,N)), respectively. Only receiving high non-scaled dosages of AuNP-BPEI would give rise to particularly high percentages of cell death ranging from around 53–88, 100, and 95–98 for hepatocytes, HUVEC, and HRPTEC, respectively, with all probable risk probabilities being considered (Figure 5(C,F,L)). On the other hand, exposure to the highest scaled dosages of AuNP-BPEI and AuNP-PEG would induce only <10% cell death, suggesting none to minimal toxicity if incorporating animal-derived HDs based on allometric scaling to the human PBPK model (Supplementary Figure S4).

**Human equivalent dose estimates**

Supplementary Table S5 summarizes the in vitro exposure concentrations causing 5% and 10% maximum cell death in four human cell types. The $E_{C5}$-derived HED estimates ranged 1.0–7.4 and 2.5–21. 1 mg/kg for hepatocytes exposed to bare AuNP-BPEI and AuNP-BPEI-HP, respectively; whereas the $E_{C10}$-derived HED estimates for hepatocytes exposed to bare AuNP-BPEI and AuNP-BPEI-HP ranged 2.1–8.0 and 4.2–43.1 mg/kg, respectively (Figure 6(A)). Furthermore, HEDs associated with PODs derived from animal studies were estimated to be 0.5, 1.4 and 0.005 mg/kg based on reported NOAEL and LOAEL for mice and LOAEL for rats, respectively (Figure 6(A)).

Besides the target organ liver, this study also estimated HEDs based on the internal concentrations in other tissues (i.e. venous plasma and kidney) as depicted in Figure 6(C). The $E_{C5}$- and $E_{C10}$-derived HEDs were estimated to be in the ranges of 2.7–4.1 and 3.3–4.6 mg/kg, respectively, based on HUVEC, and were 3.0–7.2 and 3.9–8.8 mg/kg, respectively, based on HRPTEC exposed to bare AuNP-BPEI. In addition, for HUVEC exposed to bare AuNP-PEG, the $E_{C5}$- and $E_{C10}$-derived HED estimates ranged from 1.0 to 4.5 and 2.5 to 8.2, respectively (Figure 6(C)).

**Discussion**

The present study reconstructed in vitro dose–response relationships for different types of AuNPs in selective human cells derived from different tissues or organs of healthy individuals. We also characterized AuNP external and internal exposure dosimetry based on a wide range of reported doses used in animal studies and converted into human-equivalent doses. Our analyzes suggest that for people receiving frequently applied IV doses of AuNPs from animal studies (low-to-medium range in our analysis), no or limited cytotoxicity (relative to baseline cell death) might be observed in vascular

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**Table 1.** Fitted parameters (mean ± SE) of the three- or four-parameter Hill model for reconstructing the relationship between exposure concentration and fractional cell death.

<table>
<thead>
<tr>
<th>Human cell types</th>
<th>Size/surface coating of AuNPs</th>
<th>$E_{min}$</th>
<th>$E_{max}$</th>
<th>$EC_{50}$</th>
<th>$n$</th>
<th>$r^2$</th>
</tr>
</thead>
<tbody>
<tr>
<td>Hepatocytes</td>
<td>40 nm; BPEI-HP</td>
<td>0.00001 ± 0.003</td>
<td>1</td>
<td>273.30 ± 23.36</td>
<td>2.47 ± 0.45**</td>
<td>0.95***</td>
</tr>
<tr>
<td></td>
<td>80 nm; BPEI-HP</td>
<td>0.007 ± 0.004</td>
<td>1</td>
<td>394.66 ± 5.45***</td>
<td>4.22 ± 0.28***</td>
<td>0.99***</td>
</tr>
<tr>
<td></td>
<td>40 nm; BPEI</td>
<td>0.03 ± 0.02</td>
<td>1</td>
<td>185.01 ± 7.89***</td>
<td>6.16 ± 1.86***</td>
<td>0.94***</td>
</tr>
<tr>
<td></td>
<td>80 nm; BPEI</td>
<td>0.02 ± 0.04</td>
<td>1</td>
<td>210.07 ± 15.52***</td>
<td>2.46 ± 0.57***</td>
<td>0.90***</td>
</tr>
<tr>
<td>HUVEC</td>
<td>40 nm; BPEI</td>
<td>0.006 ± 0.03</td>
<td>1</td>
<td>78.14 ± 1.68***</td>
<td>5.30 ± 0.60***</td>
<td>0.96***</td>
</tr>
<tr>
<td></td>
<td>80 nm; BPEI</td>
<td>0.008 ± 0.04</td>
<td>1</td>
<td>81.21 ± 2.30***</td>
<td>4.53 ± 0.67***</td>
<td>0.94***</td>
</tr>
<tr>
<td></td>
<td>40 nm; PEG</td>
<td>0.00001 ± 0.005</td>
<td>0.26</td>
<td>83.63 ± 23.37**</td>
<td>1.58 ± 1.01</td>
<td>0.43*</td>
</tr>
<tr>
<td>Keratinocytes</td>
<td>40 nm; BPEI</td>
<td>0.00002 ± 0.004</td>
<td>1</td>
<td>68.20 ± 4.39***</td>
<td>2.26 ± 0.27***</td>
<td>0.98***</td>
</tr>
<tr>
<td></td>
<td>80 nm; BPEI</td>
<td>0.02 ± 0.02</td>
<td>1</td>
<td>70.42 ± 2.25***</td>
<td>3.90 ± 0.34***</td>
<td>0.98***</td>
</tr>
<tr>
<td>PMNs</td>
<td>20 nm</td>
<td>0.26 ± 0.03</td>
<td>0.60</td>
<td>35.17 ± 33.14**</td>
<td>0.29 ± 0.13**</td>
<td>0.61**</td>
</tr>
<tr>
<td></td>
<td>70 nm</td>
<td>0.35 ± 0.02***</td>
<td>0.83</td>
<td>249.45 ± 112.23*</td>
<td>0.47 ± 0.13**</td>
<td>0.81***</td>
</tr>
</tbody>
</table>

BPEI: branched polyethylenimine; PEG: polyethylene glycol; $E_{min}$ and $E_{max}$: minimum and maximum fraction of cell death; $EC_{50}$: exposure concentration leading to half maximum fractional cell death (µg/ml); HP: human plasma protein; n: Hill coefficient; $r^2$: coefficient of determination.

* $E_{max} = 1$ or $E_{min} < 1$ obtains the three- or four-parameter Hill model, respectively.
* The large standard deviation was due to the dataset used. The observed maximal cell death rate was 60%, thus there was a great uncertainty from 60% to 100% cell death.

*p < 0.05; **p < 0.01; ***p < 0.001.
endothelial, liver, kidney, or skin cells. Yet, people should be aware of that extremely high cytotoxicity could occur in target organs or tissues if one received high dosages associated with those reported in rodents, even though very few animal studies have used the high dose range.

The lowest in vitro response-derived mean HED estimate of 2.7 mg/kg was around three times higher than median MAD estimate of 0.8 and comparable to median HHD estimate of 2.6 mg/kg, respectively. These results suggest that the commonly used doses in animal studies that show diagnostic, anticancer, or other therapeutic effects, if the same doses are used in humans, may cause minimal cytotoxicity. The estimated HED derived from rat study based on different toxicity endpoint (i.e. change in gene expression in liver) was 0.005 mg/kg, which is lower than the median LHD of 0.01 mg/kg. Together, these results suggest that while substantial cytotoxicity is unlikely after receiving frequently applied IV dosages of AuNPs, other subtle changes such as changes in the gene expression should not be ignored.

Even after decades of development, whether AuNPs are biocompatible and safe remains controversial. Numerous studies have reported non-toxicity or low toxicity of AuNPs (Xu et al. 2008; Simpson et al. 2013; Mannerström et al. 2016), findings consistent with the present study. Specifically, Mannerström et al. (2016) investigated cellular toxicity in mouse BALB/c 3T3 fibroblasts, rat NR8383 macrophages, as well as human U937 monocytes exposed to 13 nm citrate-coated AuNPs (0–6 µg/ml) and revealed no significant cytotoxicity. A recent in vivo study showed that 1.2 nm glutathione-coated AuNPs were biocompatible and had low immunogenicity for exposure concentration up to 60 µM in 200 µl injection per mouse (0.15 mg/kg) (Simpson et al. 2013). In particular, Xu et al. (2008) demonstrated that AuNPs (4–60 nm) did not significantly
decrease the viability of human HeLa S3 cells at exposure concentration up to 1000 μg/ml.

Jo et al. (2015) reported that although short-term AuNP toxicity was not observed in both in vitro (human intestinal epithelial cells, INT-407) and in vivo (rats) studies at a high exposure concentration or dosage of 13 μg/ml and mg/kg, potential toxicity may occur in a long-term cell proliferation assay (measured with colony-forming ability). Chen et al. (2009) suggested the long-term toxicity in mice receiving 8–37 nm AuNPs intraperitoneally at a dose of 8 mg/kg/week for 1 month with most of the mice dying before 21 days. Not dramatic but significant toxicity was demonstrated by two in vivo studies in mice with inflammation in the liver (7-day exposure) (Cho et al. 2009) and in rats with changes in the expression of hepatic genes related to detoxification, lipid metabolism, and cell cycle effects (2-month exposure) (Balasubramanian et al. 2010), respectively. While our study suggests that minimal or no toxicity may occur within 24 h after single IV exposure of commonly applied dosing levels in rodent studies, the potential toxicity after repeated or long-term exposure cannot be deemphasized and is a subject of our future studies.

None to low toxicity associated with commonly applied animal dosing levels indicated by our analyzes might result partly because of diluted internal concentrations in target tissues/organs associated with PBPK model involving biodistribution and excretion or modulated biological responses by AuNPs with HP corona formation. Previous studies
have demonstrated that AuNPs with HP corona formation could considerably attenuate cytotoxicity, proinflammatory cytokine expression, catalytic activity of cytochrome P450, and reactive oxygen/reactive nitrogen species production (Casals et al. 2010; Choi et al. 2017; Parveen et al. 2017). Following different routes of administration, NPs will be covered with different protein coronas, resulting in different biodistribution patterns and differential toxicity in varied species (Sahneh et al. 2015; Kreyling et al. 2017a, 2017b, 2017c). In addition, measured baseline values in cell death assessment may vary between different human cell types, e.g. between PMNs (Noël et al. 2016) and HUVEC (Chandran et al. 2017).

It is worthy of note that currently there is no consensus on the best method for scaling or selecting the first dose of AuNPs in humans. With potential implications of AuNPs to future therapeutic nanomedicine in humans, this study scaled frequently applied rodent dosages into human-correlated dosages (Sharma and McNeill 2009). Based
on this scaling method, our analyzed results suggest that even for people receiving the highest IV dosing levels would result in minimal cytotoxicity in hepatocytes, HUVEC, HRPTEC, and keratinocytes (Supplementary Figure S4). In comparison, extremely high cell death fraction might occur in people intravenously administered with the highest animal dosages of bare AuNP-BPEI. Yet, exposure to AuNPs with varied physicochemical characteristics, e.g. bare AuNP-PEG versus bare AuNP-BPEI, would induce differential cytotoxicity. Even though this study implies that great cytotoxicity might occur in people receiving high animal dose, none to minimal toxicity were reported from rodent studies applying high doses of AuNP-PEG or glutathione-coated AuNPs (James et al. 2007; Wong et al. 2013). Other potential toxicity effects associated with different cell types, exposure concentration, and duration by different AuNPs or different routes of exposure might exist in various species and need to be explored in future studies.

To the best of our knowledge, this is the first study integrating *in vitro* dose–response relationships based on different healthy human cell types, a validated human PBPK model, probabilistic risk assessment method, and adequate exposure reconstruction to quantitatively assess the potential toxicity risks induced by AuNPs. Recently, additional NP-related studies have incorporated PBPK modeling approach to estimate environmental and/or occupational exposure with the intention to implicate potential risk (Bachler et al. 2013, 2015; Mahapatra et al. 2015). Nevertheless, none of these studies implemented a probabilistic approach incorporating physiologically based external-to-internal dosimetric model (i.e. PBPK model) and various

Figure 6. Human equivalent doses estimated through human AuNP-PBPK model based on points of departure, including EC5 and EC10 estimated from *in vitro* as well as NOAEL and/or LOAEL from *in vivo* experimental data in liver (A), venous plasma and kidney (C). (B) Enhanced inset of (A).
toxicity endpoints to derive different PODs for biological responses in animals and humans, which is an essential element in conducting environmental and occupational risk assessment either for ecosystem or human health (Bhatt and Tripathi 2011; Kuempel et al. 2015). Stated differently, earlier studies were based solely on toxicokinetic analyzes without integrating a toxicodynamic response.

One common limitation in risk assessment when integrating multiple data sources and modeling frameworks is the uncertainty in risk estimates. This limitation also applies to the present study. To reduce uncertainty, this study employed a verified human PBPK model to describe external-to-internal dosimetry relationship. Regarding dose–response relationship, the analyzes were mostly based on in vitro toxicity data collected from the same laboratory that had very similar experimental designs and conditions, which would help reduce uncertainty. Additionally, by implementing a Bayesian-based probabilistic risk assessment approach, we were able to take the parameter variability into account to reduce potential uncertainty. Future studies that use the same NPs to conduct in vitro and in vivo toxicity, as well as PBPK modeling studies are needed in order to further reduce uncertainty in our analysis.

This present study had implemented the ISDD model (Hinderliter et al. 2010) to estimate the deposited fractions of AuNPs at different time points after exposure based on the experimental condition described in Choi et al. (2017) (Supplementary Table S2). By integrating in vitro time course data with PBPK and ISDD models, differential in vivo cytotoxicity endpoints induced by AuNPs at different exposure time scales and different levels of biology (i.e. cellular, organ, and tissue levels) could be characterized and compared with endpoints observed after in vitro exposure. However, in order to fully integrate the PBPK model with ISDD model, it is necessary to develop a more detailed mechanistic model that can simulate the concentrations of NPs at both the organ and individual cellular levels, including intracellular level. Once such multi-scale models are established, it would be possible to integrate in vitro and in vivo transcriptomics, genomics, metabolomics, as well as other toxicity time course data with the ISDD/PBPK models to conduct IVIVE and to gain more insights into the potential toxicity of NPs. In this regard, recent studies have demonstrated that it is possible to link genomics or transcriptomics data to whole-body PBPK models by integrating data from multiple sources to study mechanisms of chemical-induced toxicities (Andersen et al. 2017; Maldonado et al. 2017; Cordes et al. 2018). Our recent studies have determined the effects of AuNPs on the expression of multiple genes related to different functional pathways in different cells (Chandran et al. 2017; Choi et al. 2017). Further studies are warranted to determine the effects of AuNPs on the genomics, transcriptomics, or metabolomics in target cells or tissues, and to develop the proposed multi-scale model to better determine the potential risk of AuNPs and to elucidate the potential toxic mechanisms.

This study showed that in vitro-associated HEDs were higher than those derived from in vivo rodent studies. However, these HEDs are not directly comparable because the in vitro toxicity endpoint (e.g. cell death) is significantly different from the sub-lethal in vivo toxicity endpoints (e.g. gene expression changes in liver) and the AuNPs used in our earlier in vitro studies are different from those used in the selected in vivo studies. More in vivo as well as in vitro studies targeting the same biological response using the same type of AuNPs are urgently needed to develop and verify appropriate conversion factors with implications to interspecies extrapolation or IVIVE and to further assess the potential risk for AuNPs (Teeguarden et al. 2007; Riviere 2013; Li et al. 2017b). A PBPK model established based upon IV pharmacokinetic data may not be a suitable surrogate approach to describe pharmacokinetics after inhalational and oral uptakes (Kreyling et al. 2017a, 2017b, 2017c). Therefore, a PBPK model incorporating multiple exposure pathways is necessary to bridge environmental, occupational, or medical exposure doses and the probable magnitude in biological responses to systemically characterize potential exposure risks of AuNPs (Hirn et al. 2011; Schleh et al. 2012; Johnston et al. 2013; Kreyling et al. 2014; Riviere 2013; Bachler et al. 2013, 2015).

Conclusions
We applied a probabilistic risk assessment approach to systemically characterize AuNP exposure risks in
humans by associating a validated human PBPK model with well-established in vitro dose–response relationships. This work suggests potentially none to mild nanotoxicity for people intravenously administered with various AuNP dosages that were equivalent to the allometrically scaled or non-scaled commonly used doses in rodent studies. Based on exposure reconstructions from in vitro to in vivo extrapolation and from animal to human extrapolation, this study provides recommended AuNP administration doses that prevent people from toxicity endpoints. This study suggests that it is critical to adequately derive human equivalent doses from doses used in rodent studies for future clinical and risk assessment implications. Our computational approach provides new insights into AuNP toxicity prediction and safety evaluation in humans, an approach that could also be applied to other types of NPs.

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Disclosure statement

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